

How to understand the effects of LIPUS on bone healing? A multiscale computational investigation

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et Simulation Multi-Echelle



Ultrasound waves and living tissues

UltraSounds (US) interact with living tissues : destroy (HIFU) and repair (LIPUS)

What is LIPUS ? Low Intensity Pulsed Ultrasound Stimulation

LIPUS stimulates bone healing :

- Large literature (*Duarte 1983, Pilla et al. 1990, Heckman et al. 1994, Takikawa et al. 2000, Hemery et al. 2011, ...*)
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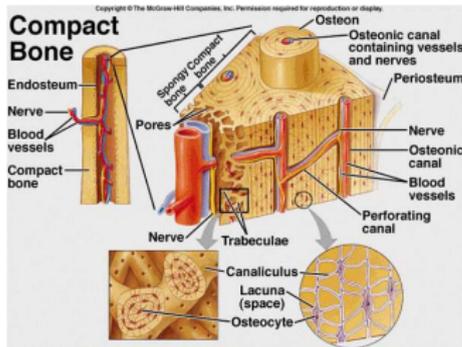
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Bone Tissue

How is cortical bone tissue organized ?



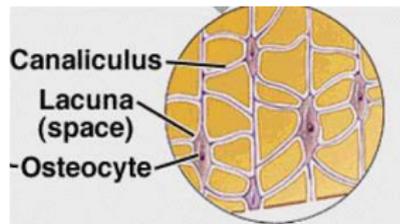
- Multiscale and two-level porosity :
Havers-Volkmann network (HV) and
lacuno-canalicular network (LCN)
- Bone cells : osteocytes
- Multiphasic (solid bone matrix, interstitial fluid
and water)

Mechanotransduction

Fluid shear stress on osteocyte

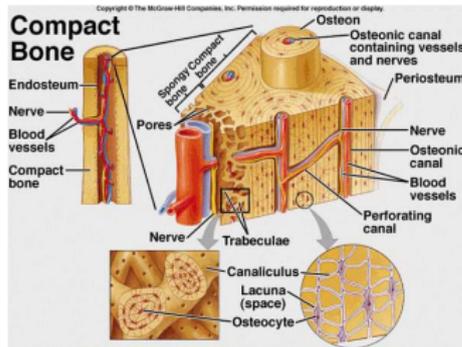
→ bone remodelling

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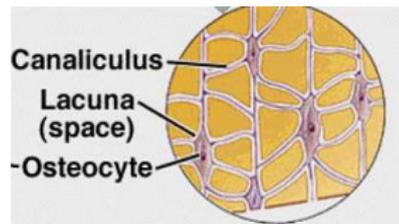
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Hypothesis : US excitation at meso-scale level induces fluid shear stress on osteocytes at micro-scale level

Locks :

- Multiscale phenomena to understand and analyze
- Multiphysics : acoustics, fluid and structure
- Coupling multiscale and multiphysics

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Development of **relevant models** to understand LIPUS mechanisms in a first **preliminary study**

Cortical bone = double-level porous medium

- vascular porosity (HV) : Havers and Volkman canals ($\varnothing \simeq 100 \mu\text{m}$)
- lacuno-canalicular network (LCN) : lacunae ($\varnothing \simeq 10 \mu\text{m}$) + canaliculi ($\varnothing < 1 \mu\text{m}$)

Biphasic medium Model : ModBone

- poroelastic bone matrix (PMB)
anisotropic solid (*Scheiner et al. 2015*) + LCN
→ equivalent medium (Biot's model)
- HV pores = fluid phase

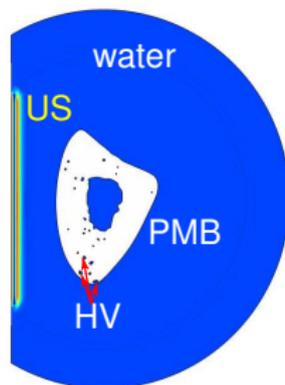
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Osteocyte Model : ModOst

- Osteocyte cell (solid phase)
- Interstitial Fluid (IFluid) (fluid phase)
- Extracellular matrix, ECM (solid phase)

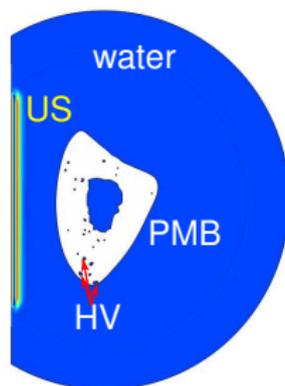
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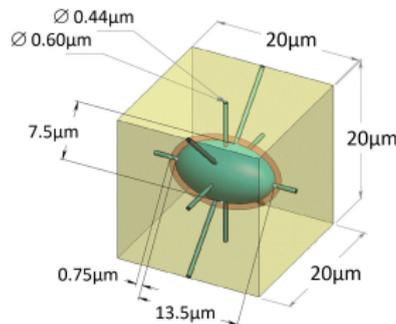
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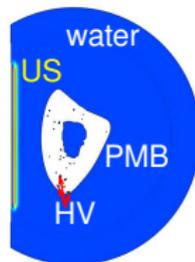


2D and 3D coupling between acoustics and fluid and fluid-solid interaction Software : Comsol Multiphysics

- ModBone (2D) : US stimulation at the mesoscale
HV from CT scan images ($22.5 \mu\text{m}$)
Time-dependent problem
Weak form of wave propagation in poroelastic medium
(Nguyen et al. 2010)
 $\Delta x_{\text{bone}} \approx 0.7 \text{ mm}$, $\Delta x_{\text{water}} \approx 0.4 \text{ mm}$ and $\Delta t \approx 0.1 \mu\text{s}$
→ 40h to simulate a single cycle propagation.

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► input parameters :

US stimulation parameters (from Exogen device)

$f=1\text{MHz}$, pressure=2kPa, duty cycle=20%, pulse duration=1ms, \varnothing transducer=10mm

surrounding fluid properties = water

bone material properties = anisotropic poroelasticity (*Scheiner et al. 2015, Goulet et al. 2008, Nguyen et al. 2010, Cowin et al. 2009*)

► output parameter : |Fluid pressure gradient|

FE simulation

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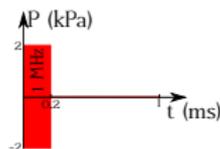
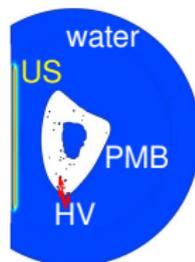
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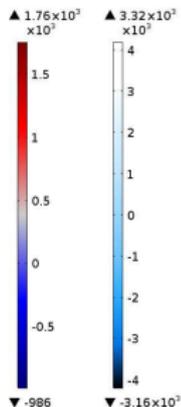
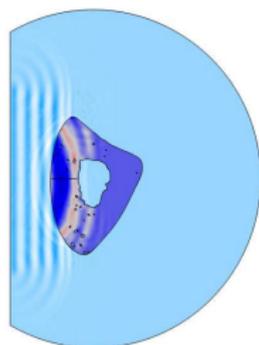
- ▶ output parameter : **IFluid pressure gradient**



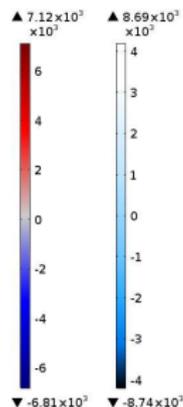
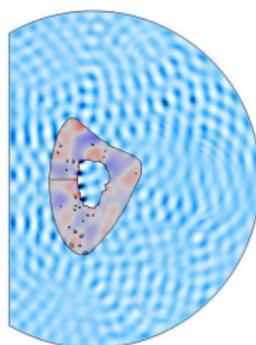
Results and Discussion : ModBone

Acoustic pressure and IFluid pressure (Pa)

t = 4 μ s



t = 20 μ s



- IFluid pressure (IFluid P) difference induced by US stimulation on 1 cycle

$$\text{Max}|\text{IFluid P}_{\text{periosteum}} - \text{IFluid P}_{\text{endosteum}}| \approx 15000 \text{ Pa}$$

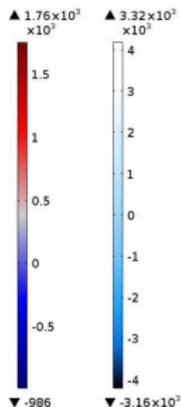
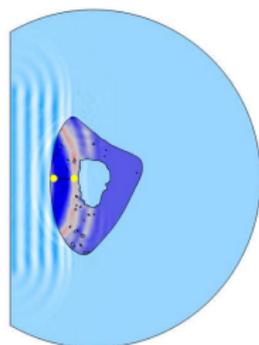
$$\rightarrow \text{IFluid P gradient} = 5 \text{ Pa}/\mu\text{m}$$

- IFluid P gradient $\approx 30 \text{ Pa}/\mu\text{m}$ (Anderson et al. 2005, Verbruggen et al. 2012, 2014)
→ 6-times lower than previous studies considering physiological mechanical loading.
- Fluid shear stress on osteocyte?

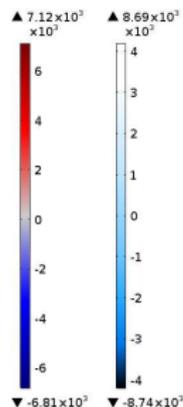
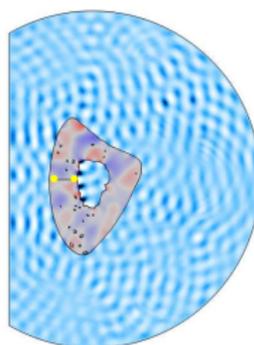
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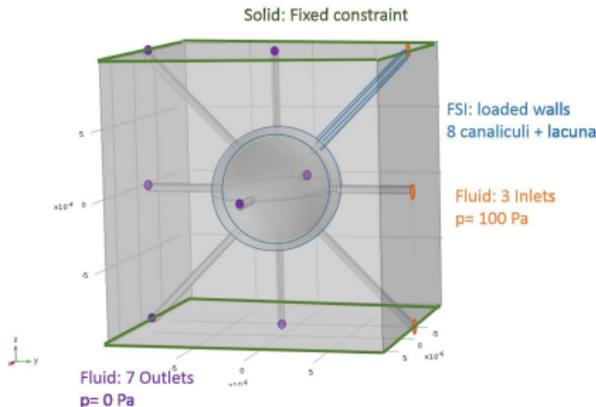
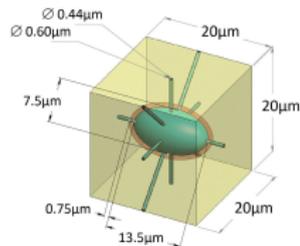
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● ModOst (3D) : Fluid Structure Interaction Model (one-way coupling)

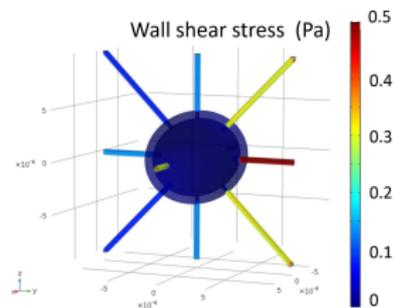
- ▶ input parameters : IFluid P gradient from ModBone : $5 \text{ Pa}/\mu\text{m}$
- ▶ output parameters : fluid shear stress on osteocyte : τ



IFluid domain : newtonian,
 $\rho = 997 \text{ kg/m}^3$,
 $\mu = 885 \times 10^{-4} \text{ kg.m}^{-1} \cdot \text{s}^{-1}$

Solid domain : linear elastic,
ECM : $E = 16.6 \text{ GPa}$, $\nu = 0.38$;
osteocyte : $E = 4.47 \text{ kPa}$, $\nu = 0.3$

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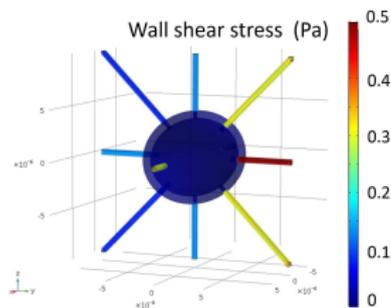


Fluid shear stress on osteocyte
(cell body and processes)

$$\tau_{max} \approx 0.8 \text{ Pa}$$

- Shear stress patterns obviously related to simple symmetrical geometry and boundary conditions
- Theoretical shear stress interval for osteocyte activation : 0.8-3 Pa (*Weinbaum et al. 1994*)
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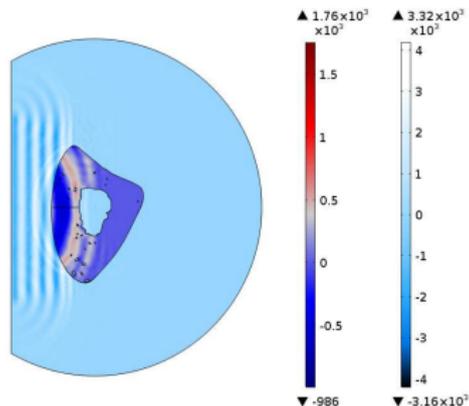
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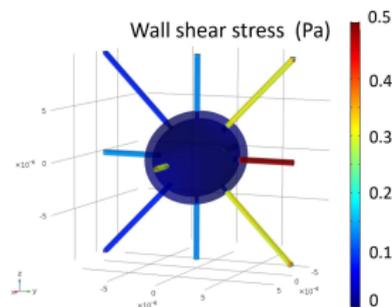
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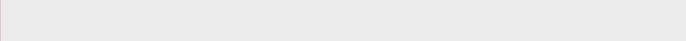


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Thank you for your attention.
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carine.guivier@univ-amu.fr



Poroelastic bone properties

Transverse isotropic extralacunar matrix

$$\begin{pmatrix} 22.88 & 8.93 & 10.14 & 0 & 0 & 0 \\ 8.93 & 22.88 & 10.14 & 0 & 0 & 0 \\ 10.14 & 10.14 & 29.60 & 0 & 0 & 0 \\ 0 & 0 & 0 & 14.72 & 0 & 0 \\ 0 & 0 & 0 & 0 & 14.72 & 0 \\ 0 & 0 & 0 & 0 & 0 & 13.96 \end{pmatrix} \text{ (GPa)}$$

(Scheiner et al. 2015)

Mass density : $\rho=1.9 \text{ g/cm}^3$

Isotropic LCN permeability : $2.2 \times 10^{-22} \text{ m}^2$ *(Smith et al. 2002, Cowin et al. 2009)*

Other Biot's parameters from *NGuyen et al. 2016*

Mesh

