

ESUCB 2011



Characterization of growing bone : curvature and anisotropy.

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21 juin 2011

Outline

1 Characteristics of growing bone

- Geometry
- Anisotropy
- FGM

2 Bone model

- Anisotropy & tube
- US characterization

3 Results

- Plate or tube
- Influence of soft tissue

4 Conclusion

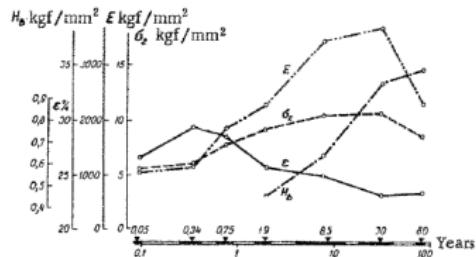
Mechanical behaviour : what about literature ?

- Few studies about the properties of human growing bone :

- Mechanical properties

Currey and Butler (JB&JS, 1975) : stiffness and toughness of children bone 30% lower than adult bone.

Vinz (Mechanics Of Composite Materials, 1975)



- Microstructural properties

Kerley (American Journal of Physical Anthropology, 1965)

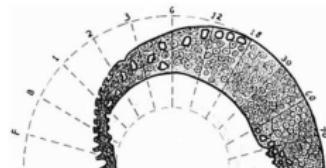


Fig. 2a Cross-sectional age changes in the femoral cortex.

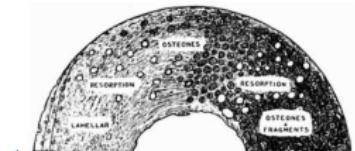


Fig 2b The life cycle of bone.

- Berteau et al. *Elastic values of fibula children bone autotransplants* ESUCB 2011

(Mon 20 June 2011, 10 :45-11 :00)

Specificity of growing bone : geometry

Long bone \approx tubular geometry

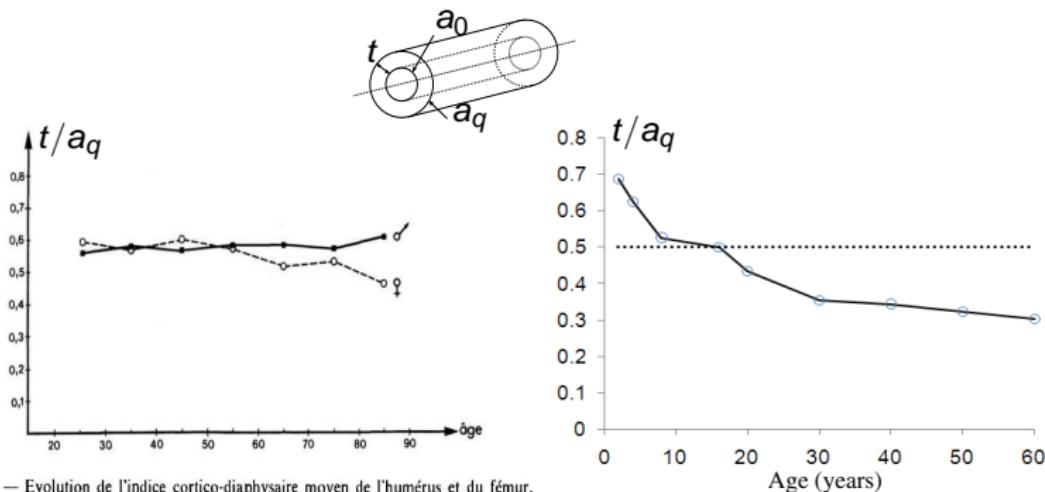


FIG. 6. — Evolution de l'indice cortico-diaphysaire moyen de l'humérus et du fémur, en fonction de l'âge, par classes décennales.

Bergot & Bocquet (1976)

Carter & Beaupré (2001)

Hypothesis

- Lack of data in literature on healthy children bone

⇒ hypothesis on anisotropy.

growing bone = less organized bone : orthotropy vs transverse isotropy.

Ex. plexiform bone = immature bone in quickly growing animals ⇒ orthotropic (Katz, 1984)

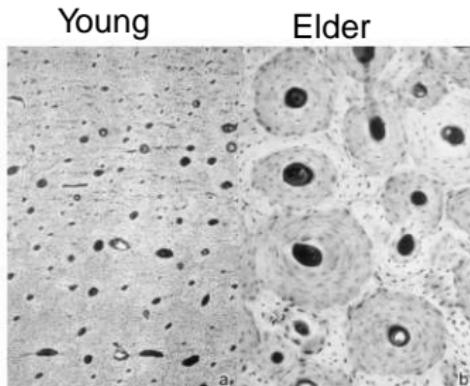


Fig. 4. A light microscopic image of Villanueva's bone stain from a young aged sample (a) and from an older aged sample (b). Various osteons appear in the older, but not in the young.

Watanabe et al. (1998)

Hypothesis

FGM=Functionally Graded Material = determinant of aging and pathology ?

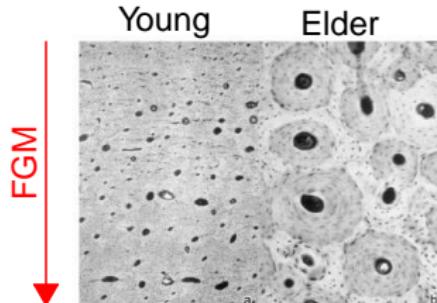


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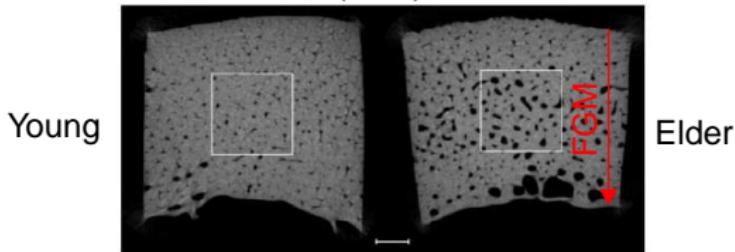


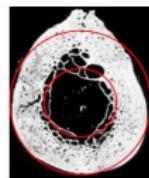
Figure 2. Two-dimensional cross-sectional micro-computed tomography Images from samples A (left) and B (right) acquired at 10 μm spatial resolution. The region of interest represents the region of interest ($2.5 \text{ mm} \times 2.5 \text{ mm}$) targeted for skeletonization and quantitative analysis. Scale bar = 1 mm.

Cooper et al. (2003)

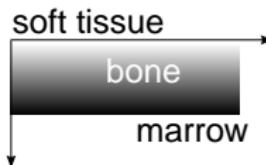
How to model bone ?

Clinical application → *in-vivo* model

- Geometry
 - ▶ plate
 - ▶ cylinder
 - ▶ tube
 - ▶ realistic section
- Boundary conditions
 - ▶ vacuum(free-free)
 - ▶ fluid (soft tissue and marrow) : perfect fluids or viscous fluids
- Properties of bone
 - ▶ elasticity/visco-elasticity
 - ▶ linear/non-linear elasticity
 - ▶ isotropy/anisotropy
 - ▶ homogeneity/heterogeneity



Baron Ultrasonics 2011.

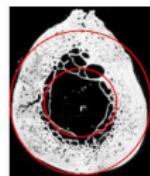


Baron et al. CRM (2008);
Baron et al. JASA (2010).

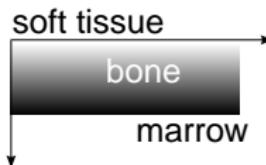
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Characterization of an anisotropic tube

Anisotropy
 (> transverse isotropy)
 +
cylindrical geometry
 +
 FGM

→ Classical methods
 inefficient
 (no analytical solution)

→ Stroh's formalism
 (Peano series expansion
 of the matricant)

Wave equation in Fourier domain : $\frac{d}{dr}\eta(r) = \mathbf{Q}(r)\eta(r).$

with $\eta(r) = (u_r, u_\theta, u_z, ir\sigma_{rr}, ir\sigma_{r\theta}, ir\sigma_{rz})^T$ and $\mathbf{Q} = \mathbf{Q}(\mathbf{C}, k, \omega).$

Analytic solution : Peano expansion of the matricant

$$\mathbf{M}(r, r_0) = \mathbf{I} + \int_{r_0}^r \mathbf{Q}(\xi) d\xi + \int_{r_0}^r \mathbf{Q}(\xi) \int_{r_0}^\xi \mathbf{Q}(\xi_1) d\xi_1 d\xi + \dots,$$

$\mathbf{M}(r, r_0)$ is a propagator matrix :

$$\eta(a_q) = \mathbf{M}(a_q, a_0)\eta(a_0)$$

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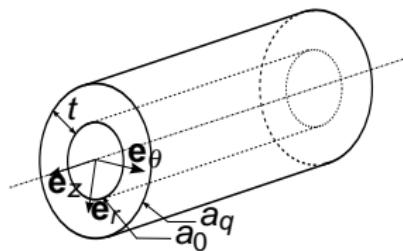
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Tube in vacuum → eigenmodes



- axial waves
 - ▶ longitudinal modes $L(0, m)$
 - ▶ torsionnal modes $T(0, m)$
 - ▶ flexural modes $F(n, m)$
- circumferential waves

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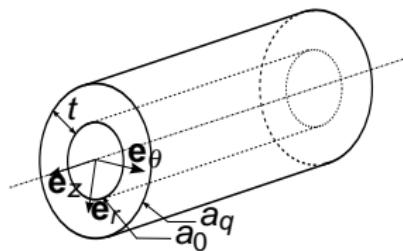


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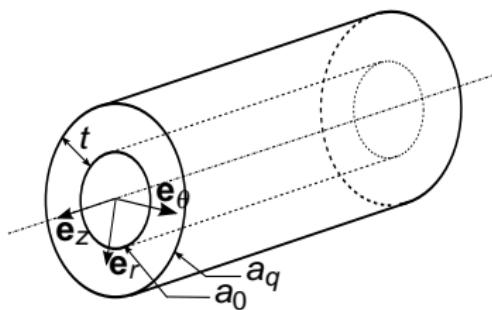


- **axial waves**

- ▶ longitudinal modes $L(0, m)$
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- ▶ flexural modes $F(n, m)$

- **circumferential waves**

Plate vs. tube

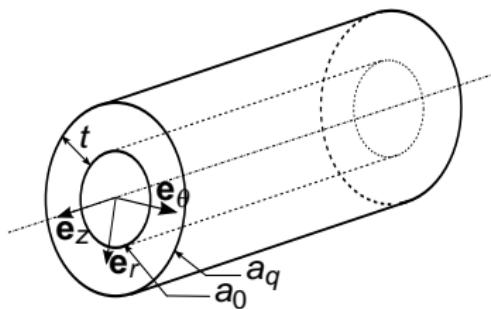


$t/a_q < 0.5$ → Plate - SH and Lamb waves

$t/a_q > 0.5$ → Tube - axial waves

Cortical bone : anisotropic tube.

Plate vs. tube



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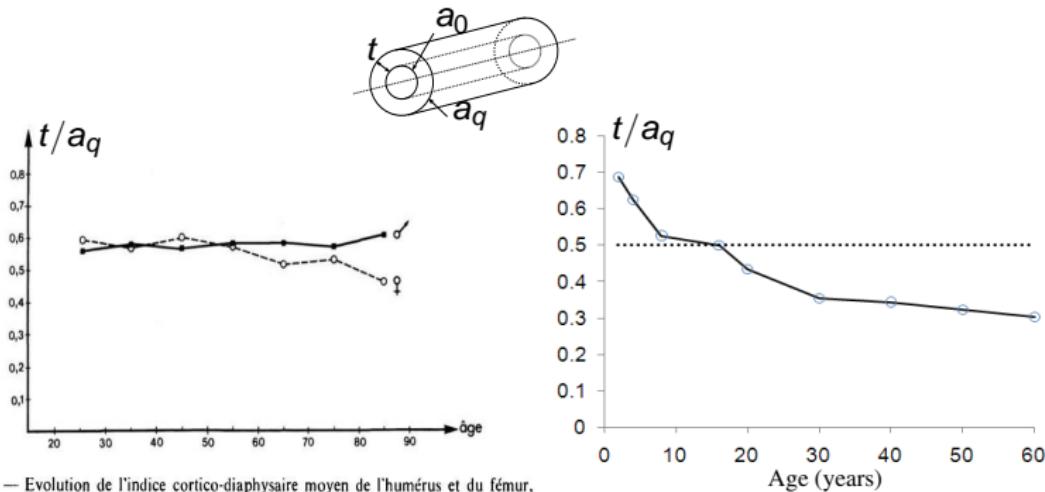


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Bone properties

Orthotropic material

$$\begin{pmatrix} 18 & 9.98 & 10.1 & 0 & 0 & 0 \\ 9.98 & 20.2 & 10.7 & 0 & 0 & 0 \\ 10.1 & 10.7 & 27.6 & 0 & 0 & 0 \\ 0 & 0 & 0 & 6.23 & 0 & 0 \\ 0 & 0 & 0 & 0 & 5.61 & 0 \\ 0 & 0 & 0 & 0 & 0 & 4.52 \end{pmatrix}$$

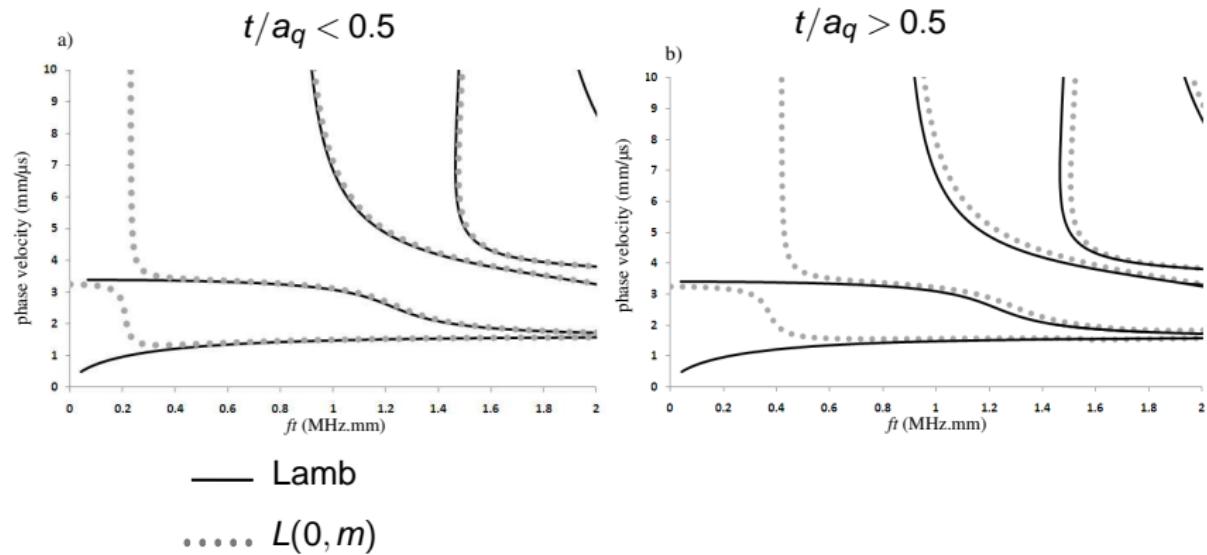
Van Burskirk & Ashman, 1981

Long bone : plate or tube

- Dispersion curves of propagation modes :
 - plate
 - tube
- 2 ratios : $t/a_q = 0.4 < 0.5$ et $t/a_q = 0.6 > 0.5$
- modes
 - ▶ longitudinal
 - ▶ torsional
 - ▶ flexural

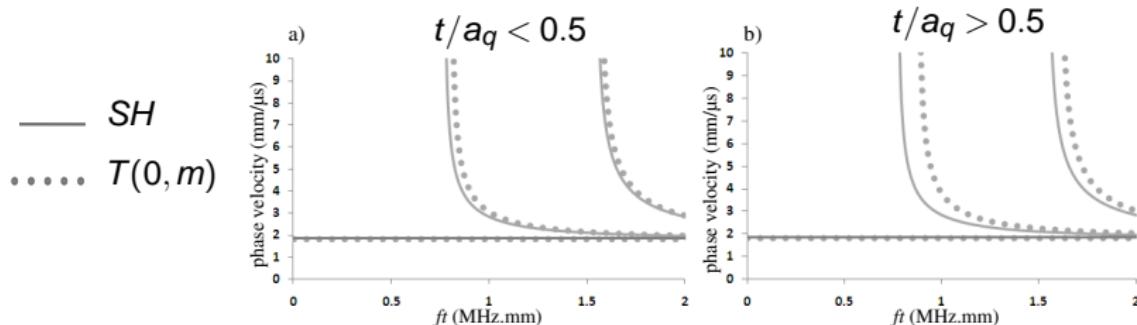
Long bone : plate or tube

longitudinal modes



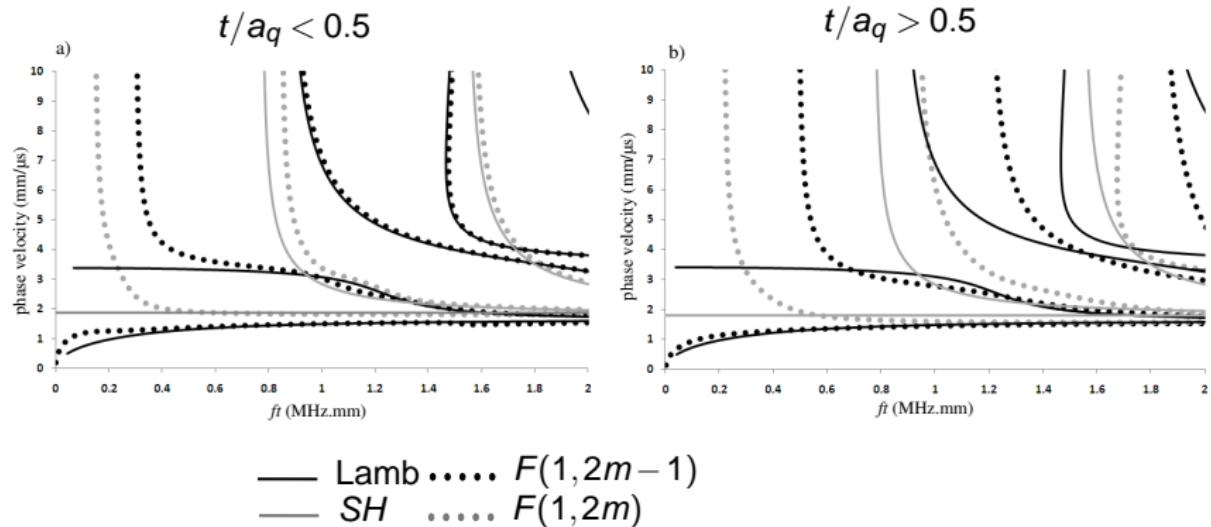
Long bone : plate or tube

torsional modes



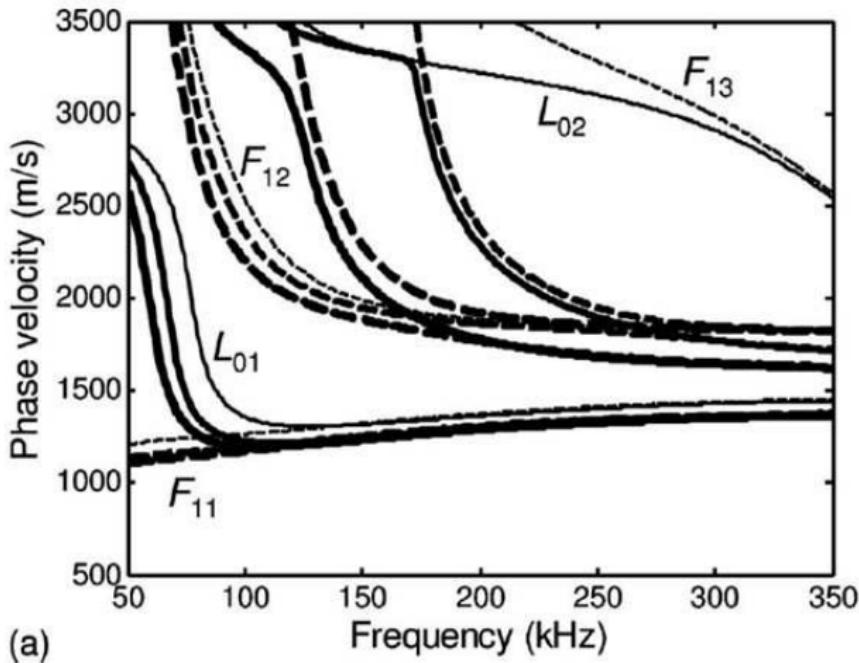
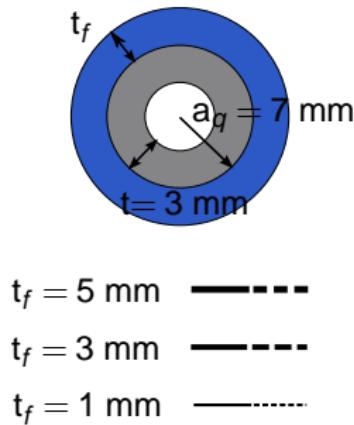
Long bone : plate or tube

flexural modes



Soft Tissue

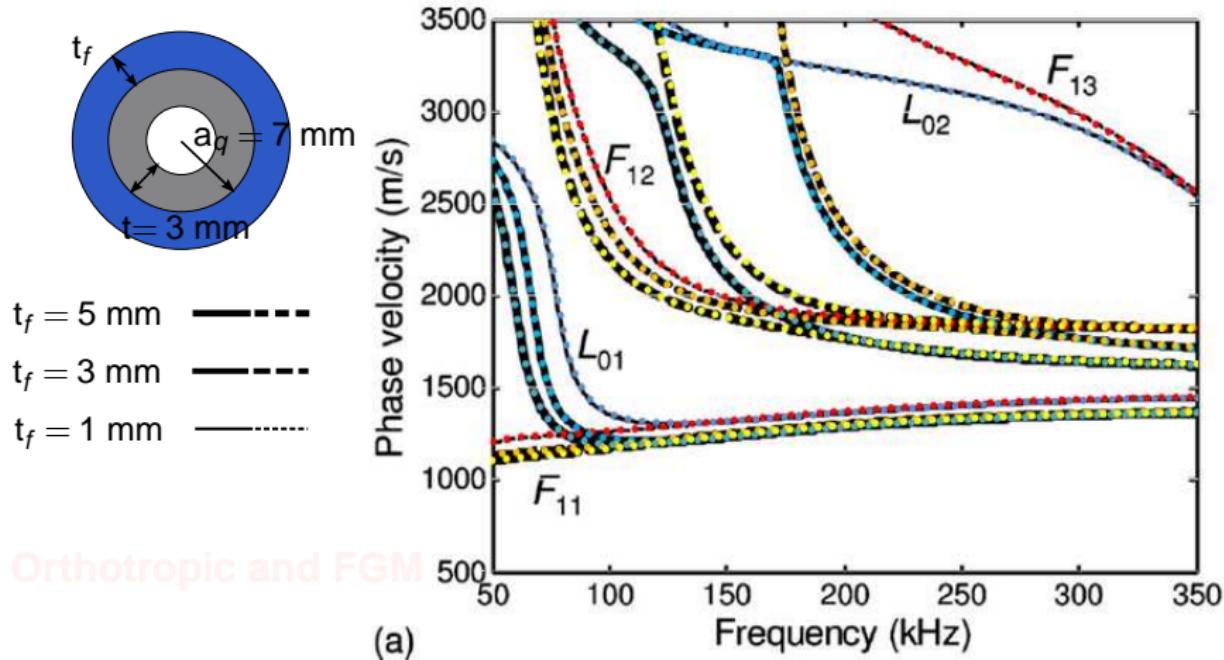
Isotropic bone tube coated with water shell (Moilanen et al., JASA 2008)



(a)

Soft Tissue

Isotropic bone tube coated with water shell (Moilanen et al., JASA 2008)

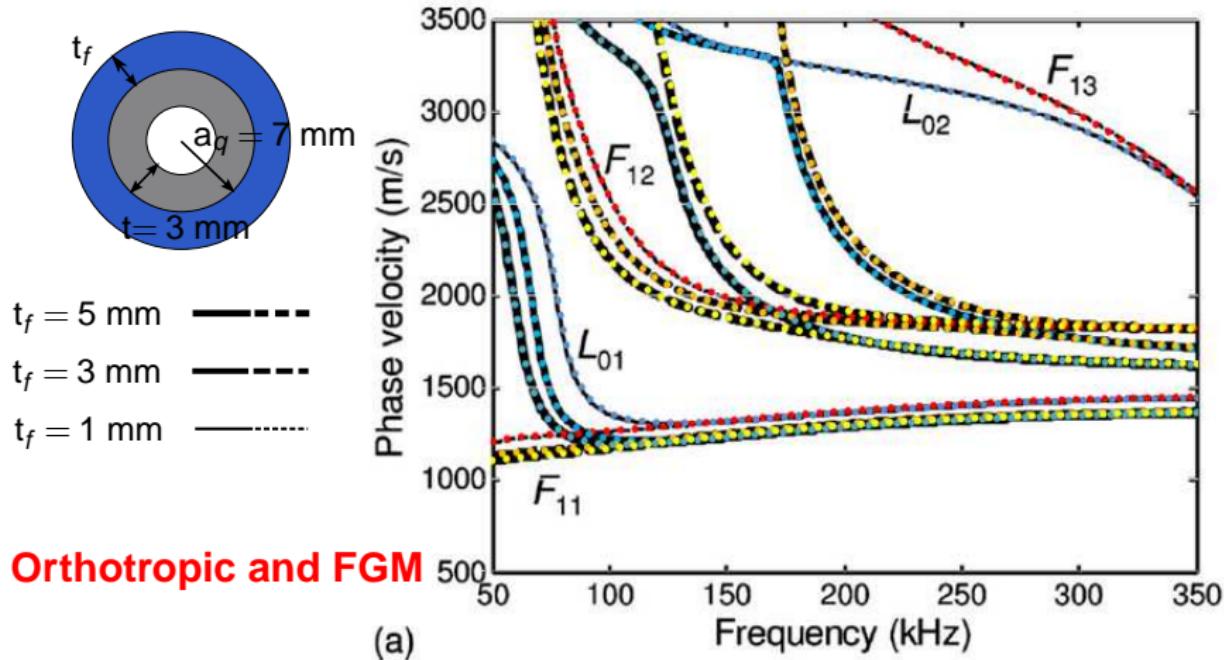


Orthotropic and FGM

(a)

Soft Tissue

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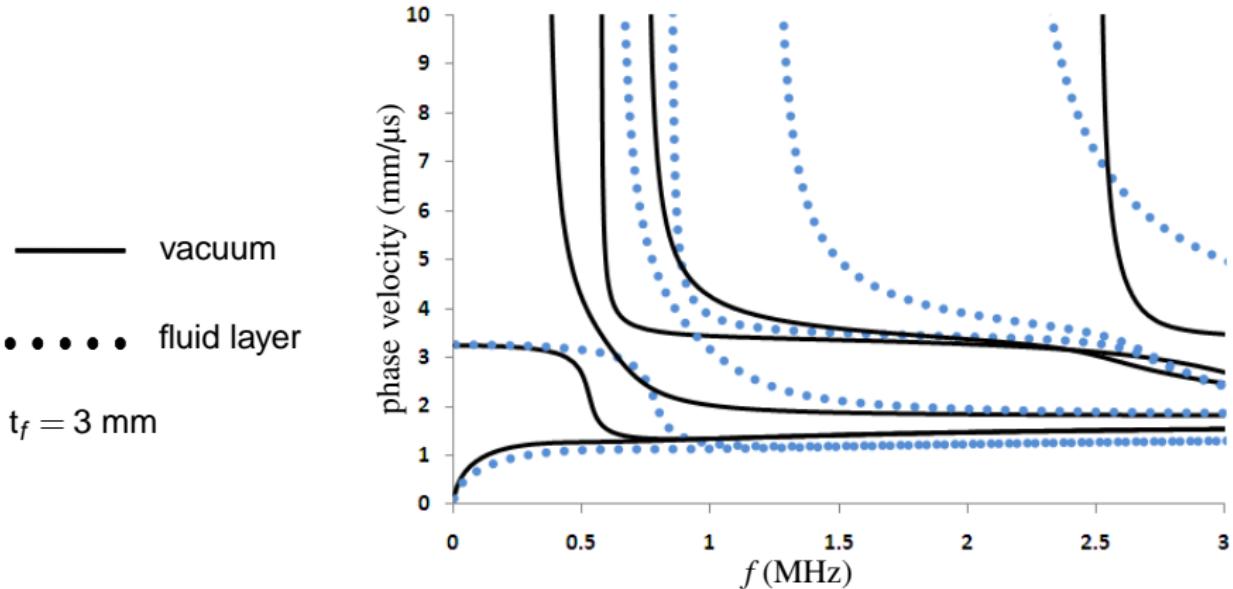


Orthotropic and FGM

Soft Tissue

Orthotropic bone tube

free-free (black solid lines) and coated with water shell (blue dots)



Conclusion and perspectives

- Analytical solution (Peano expansion of the matricant - Stroh's formalism)
⇒ Guided waves propagation in an **orthotropic functionnally graded** tube coated by a perfect fluid layer
- Further work
Fill the tube ⇒ problem of infinite values for $r \ll 1$.

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Fill the tube ⇒ problem of infinite values for $r \ll 1$.

Thank you !

Equation

$$\mathbf{Q}(r) = \frac{1}{r} \begin{pmatrix} -\frac{c_{12}}{c_{11}} & -in\frac{c_{12}}{c_{11}} \\ -in & 1 \\ -ik_z r & 0 \\ in(\gamma_{12} - r^2 \rho \omega^2) & -n\gamma_{12} \\ n\gamma_{12} & in^2 \gamma_{12} + ir^2 (k_z^2 c_{44} - \rho \omega^2) \\ k_z r \gamma_{23} & ink_z r (\gamma_{23} + c_{44}) \\ \\ -ik_z r \frac{c_{13}}{c_{11}} & -\frac{i}{c_{11}} & 0 & 0 \\ 0 & 0 & -\frac{i}{c_{66}} & 0 \\ 0 & 0 & 0 & \frac{i}{c_{65}} \\ \dots & -k_z r \gamma_{23} & \frac{c_{12}}{c_{11}} & -in & -ik_z r \\ ink_z r (\gamma_{123} + c_{44}) & -in \frac{c_{12}}{c_{11}} & -1 & 0 \\ in^2 c_{44} + ir^2 (k_z^2 \gamma_{13} - \rho \omega^2) & -ik_z r \frac{c_{13}}{c_{11}} & 0 & 0 \end{pmatrix}$$

with

$$\gamma_{12} = c_{22} - \frac{c_{12}^2}{c_{11}} ; \gamma_{13} = c_{33} - \frac{c_{13}^2}{c_{11}} ; \gamma_{23} = c_{23} - \frac{c_{12} c_{13}}{c_{11}}$$

Propriétés de l'os

	c_{11} (GPa)	c_{13} (GPa)	c_{33} (GPa)	c_{44} (GPa)	c_{66} (GPa)	ρ (g.cm $^{-3}$)
C_M	25.9	11.1	29.6	5.5	4.4	1.753
C_m	11.8	5.1	17.6	3.3	2.2	1.66

TABLE: Les valeurs minimale et maximale [C_m, C_M] de chaque propriété avec $c_{12} = c_{11} - 2c_{66}$. A noter que la correspondance entre les directions de l'espace et la notation indicelle est $1 \leftrightarrow r; 2 \leftrightarrow \theta; 3 \leftrightarrow z$.

Profil linéaire

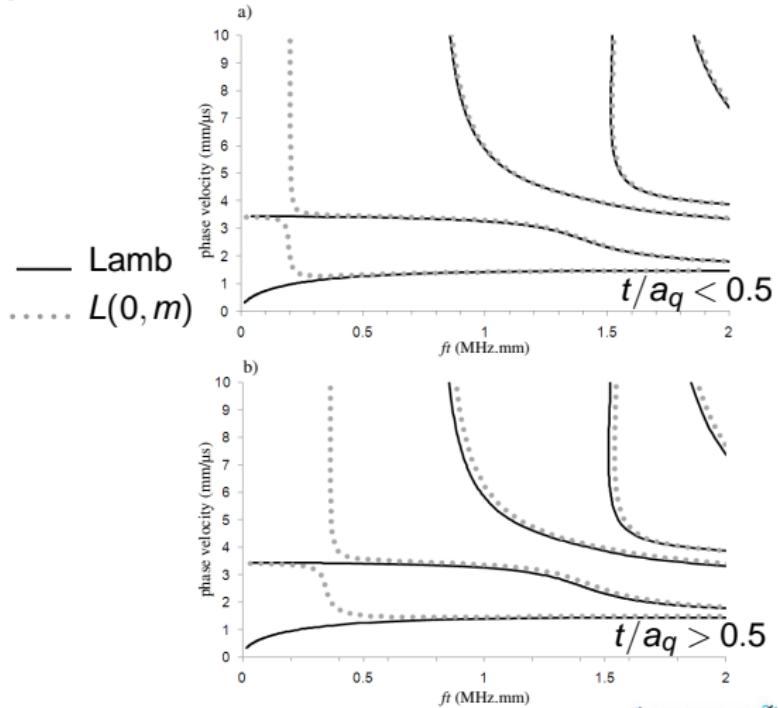
$$C(r) = C_m + (C_M - C_m)(r - a_0)/(a_q - a_0),$$

L'os : plaque ou tube

- Courbes de dispersion des modes de propagation :
 - plaque
 - tube
- 2 rapports : $t/a_q = 0.4 < 0.5$ et $t/a_q = 0.6 > 0.5$
- modes
 - ▶ longitudinaux
 - ▶ de torsion
 - ▶ de flexion

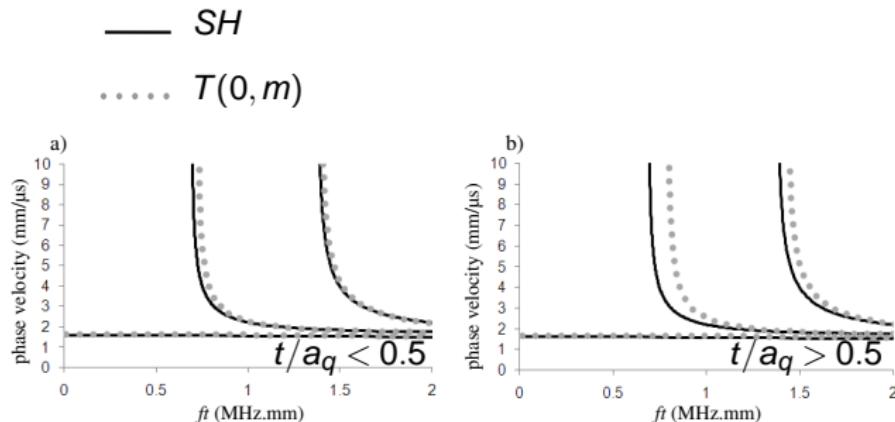
L'os : plaque ou tube

modes longitudinaux



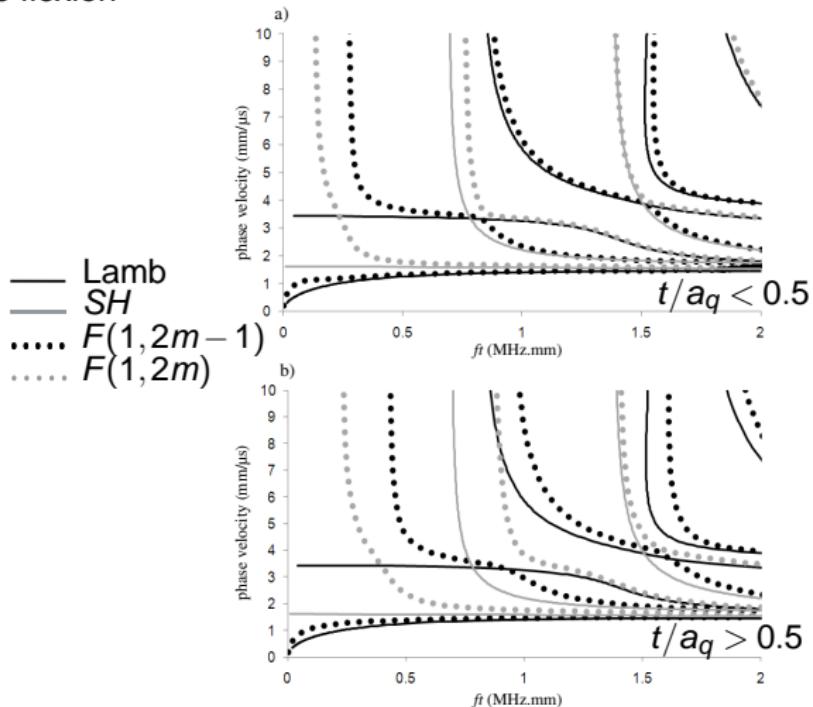
L'os : plaque ou tube

modes de torsion



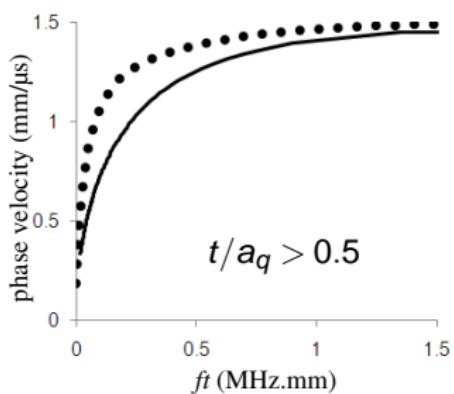
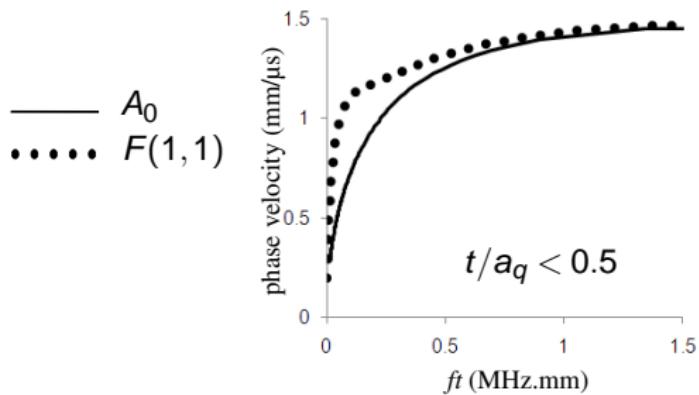
L'os : plaque ou tube

modes de flexion



Estimation de l'épaisseur corticale : A_0 vs $F(1,1)$

Dans Moilanen et al., UMB (2007) : estimation de l'épaisseur corticale
 A_0 vs $F(1,1)$



Baron, Ultrasonics (2011)