

Interaction of ultrasound with cortical bone as a two-level porous medium: a multiscale computational study.

Cécile Baron¹, Carine Guivier-Curien², Vu-Hieu Nguyen³, Salah Naili³

¹Aix-Marseille Université, CNRS, ISM UMR 7287, Marseille France

²Aix-Marseille Université, CNRS, Ecole Centrale, IRPHE UMR 7342, Marseille France

³Université Paris Est, MSME UMR 8208 CNRS, Créteil France

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et Simulation Multi Echelle



Ultrasound waves and living tissues

UltraSounds (US) interact with living tissues : destroy (HIFU) and repair (LIPUS)

What is LIPUS ? Low Intensity Pulsed Ultrasound Stimulation

LIPUS stimulates bone healing :

- Large literature (*Duarte 1983, Pilla et al. 1990, Heckman et al. 1994, Takikawa et al. 2000, Hemery et al. 2011, ...*)
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But how ?

Open question !

(Claes et al. 2007, Padilla et al. 2014)

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Bone Tissue

- trabecular bone = spongy bone
- **cortical bone** = compact bone

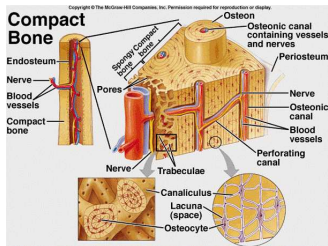
How is cortical bone tissue organized ?

- Porous and multiscale :
 - ▶ vascular porosity (HV) :
Havers and Volkman canals ($\varnothing \simeq 100 \mu\text{m}$)
 - ▶ lacuno-canalicular network (LCN) :
lacunae ($\varnothing \simeq 10 \mu\text{m}$) + canaliculi ($\varnothing < 1 \mu\text{m}$)
- Bone cells : osteocytes

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Mechanotransduction

Fluid shear stress on osteocyte \rightarrow bone remodelling

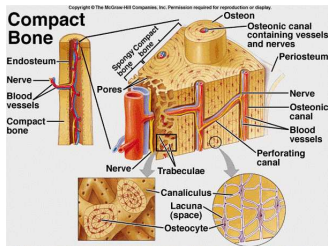
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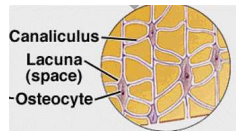


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Cortical bone = double-level porous medium

Hypothesis : US excitation at meso-scale level induces fluid shear stress on osteocytes at micro-scale level

Locks :

- Multiscale phenomena to understand and analyze
- Multiphysics : acoustics, fluid and structure
- Coupling multiscale and multiphysics

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Models

Biphasic medium Model + US : ModBone

- Vascular pores (HV) = fluid phase
HV pores reconstructed from binarized μ CT images (22.5 μ m)
- Poroelastic bone matrix (PBM)
anisotropic solid (*Scheiner et al. 2015*) + LCN \rightarrow equivalent medium (Biot's model)

RX image

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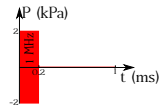
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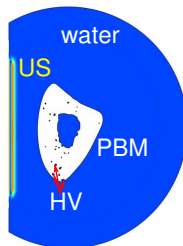
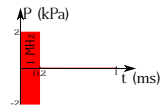
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Osteocyte Model : ModOst

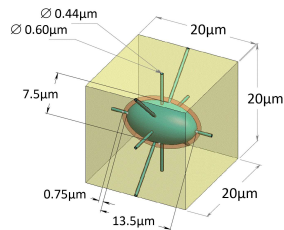
- Osteocyte cell (solid phase)
- Extracellular matrix, ECM (solid phase)
- Interstitial Fluid (IFluid) (fluid phase)

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2D and 3D coupling between acoustics and fluid and fluid-solid interaction Software : Comsol Multiphysics

- ModBone (2D) : US stimulation at the mesoscale
Time-dependent problem
Weak form of wave propagation in poroelastic medium
+ boundary conditions

(Nguyen et al. 2010)

$\Delta x_{\text{bone}} \approx 0.7 \text{ mm}$, $\Delta x_{\text{water}} \approx 0.4 \text{ mm}$ and $\Delta t \approx 0.1 \mu\text{s}$
→ 40h to simulate a single cycle propagation.

FE simulation

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US stimulation parameters from Exogen device

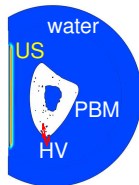
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surrounding fluid properties = water

bone material properties = anisotropic poroelasticity

(*Scheiner et al. 2015, Goulet et al. 2008, Nguyen et al. 2010, Cowin et al. 2009*)

► output parameter : IFluid pressure gradient



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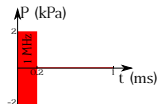
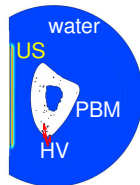
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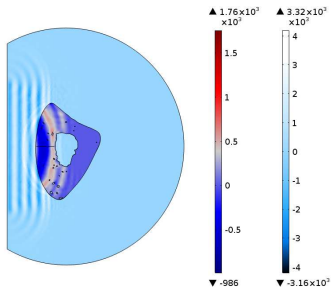
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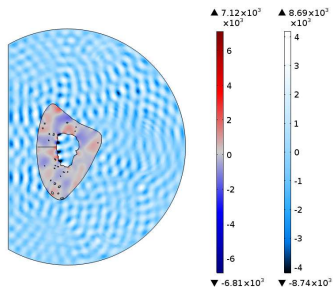
Results and Discussion : ModBone

Acoustic pressure and IFluid pressure (Pa)

$t = 4 \mu s$



$t = 20 \mu s$



- IFluid pressure (IFluid P) difference induced by US stimulation on 1 cycle

$$\text{Max}|\text{IFluid P}_{\text{periosteum}} - \text{IFluid P}_{\text{endosteum}}| \approx 11000 \text{ Pa}$$

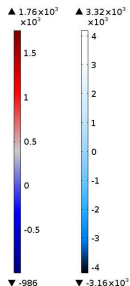
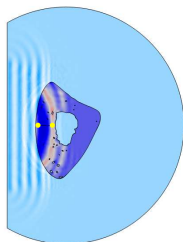
$$\rightarrow \text{IFluid P gradient} = 3.8 \text{ Pa}/\mu\text{m}$$

- IFluid P gradient $\approx 30 \text{ Pa} / \mu\text{m}$ (Anderson et al. 2005, Verbruggen et al. 2012, 2014)
 \rightarrow 8-times lower than previous studies considering physiological mechanical loading.
- Fluid shear stress on osteocyte?

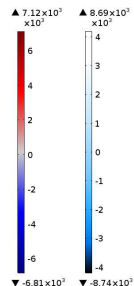
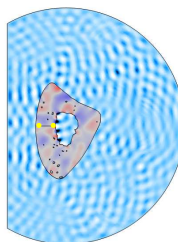
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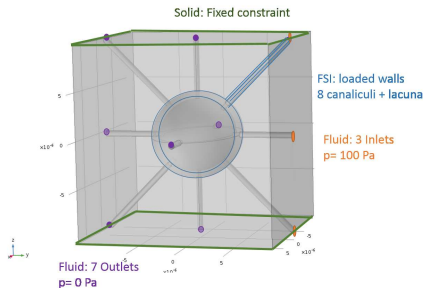
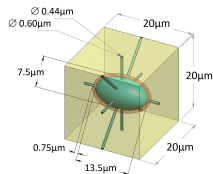
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- ModOst (3D) :

Fluid Structure Interaction Model (one-way coupling)

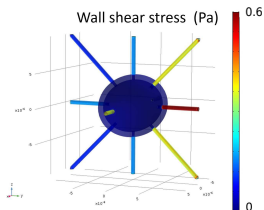
- ▶ input parameter : IFluid P gradient from ModBone : $3.8 \text{ Pa}/\mu\text{m}$
- ▶ output parameter : fluid shear stress on osteocyte : τ



IFluid domain : newtonian,
 $\rho=997 \text{ kg/m}^3$,
 $\mu=885 \times 10^{-4} \text{ kg.m}^{-1}.\text{s}^{-1}$

Solid domain : linear elastic,
ECM : $E=16.6$ GPa, $\nu=0.38$;
osteocyte : $E=4.47$ kPa, $\nu=0.3$

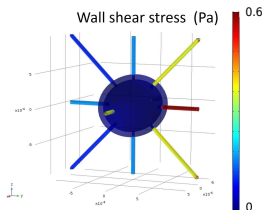
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(cell body and processes)
 $\tau_{max} \approx 0.6 \text{ Pa}$

- Shear stress patterns obviously related to simple symmetrical geometry and boundary conditions
- Theoretical shear stress interval for osteocyte under physiological load : 0.8-3 Pa (*Weinbaum et al. 1994*)
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 - ▶ LCN permeability $2.2 \times 10^{-22} \text{ m}^2$ (Cowin *et al.* 2009)
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- On-going modelling
 - ▶ **ModBone** : permeability of endosteum, mechanical properties of healing tissues and US parameters, 3D
 - ▶ **ModOst** : 3D osteocyte network, pericellular space and oscillatory interstitial fluid

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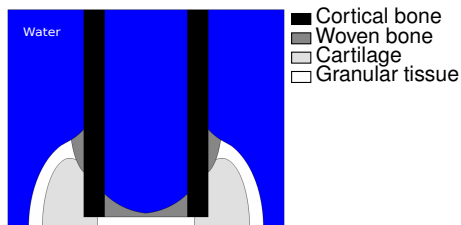
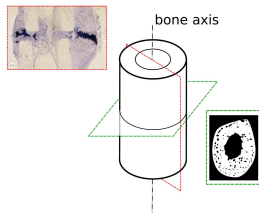
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Bone callus model

- geometry
- healing tissues properties



Bailon-Plaza et al. 2001, Claes et Heigele 1999

Vascular porosity ?

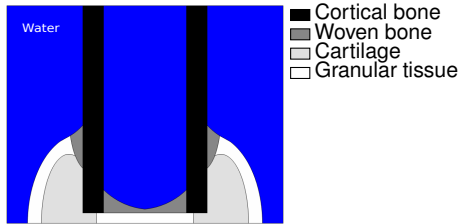
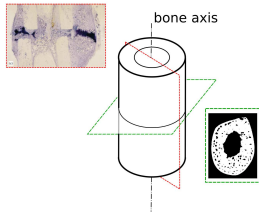
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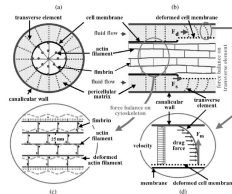


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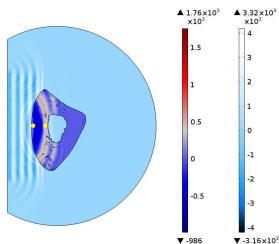
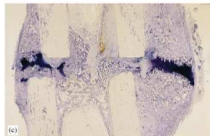
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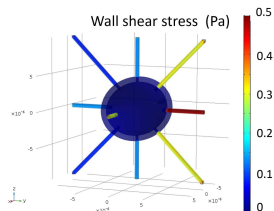
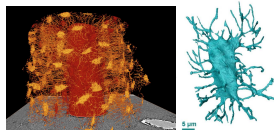
You et al. 2001

Conclusion and Perspectives

Tissue scale

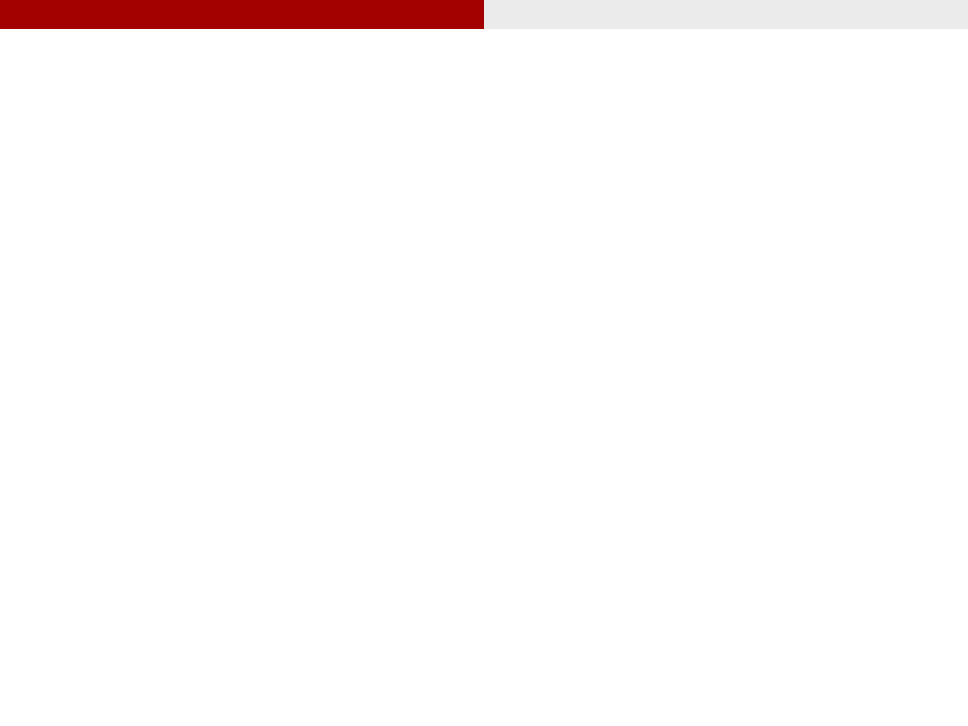


Microscopic scale



Thank you for your attention.
Any questions (or answers) ?

cecile.baron@univ-amu.fr
carine.guivier@univ-amu.fr



Equations

- Wave propagation in the anisotropic poroelastic matrix (from *Nguyen et al. 2012*)

The constitutive equations for the anisotropic linear poroelastic material are given by

$$\boldsymbol{\sigma} = \mathbb{C} : \boldsymbol{\epsilon} - \boldsymbol{\alpha} p, \quad (7)$$

$$-\frac{1}{M} p = \nabla \cdot \mathbf{w} + \boldsymbol{\alpha} : \boldsymbol{\epsilon}, \quad (8)$$

where $\mathbb{C}(\mathbf{x})$ is the elasticity fourth-order tensor of drained porous material; $\boldsymbol{\alpha}$, which is a symmetric second-order tensor, is the Biot effective tensor; M is the Biot scalar modulus; $\boldsymbol{\epsilon}(\mathbf{x}, t)$ is the infinitesimal strain tensor, which is defined as the symmetric part of $\nabla \mathbf{u}^s$.

$$\mathbf{w} = \phi(\bar{\mathbf{u}}^f - \mathbf{u}^s)$$

- boundary conditions : pressure and stress fields continuity + *open pore* condition (continuity of the normal relative velocity between fluid and solid)

Poroelastic cortical bone properties

Transverse isotropic extralacunar matrix

$$\begin{pmatrix} 22.88 & 10.14 & 0 \\ 10.14 & 29.60 & 0 \\ 0 & 0 & 6.98 \end{pmatrix} (GPa)$$

(Scheiner et al. 2015)

Mass density : $\rho=1.9 \text{ g/cm}^3$

Isotropic LCN permeability : $2.2 \times 10^{-22} \text{ m}^2$ (Smith et al. 2002, Cowin et al. 2009)

Other Biot's parameters from NGuyen et al. 2016

$\phi=5\%$, $\alpha_1=0.11$, $\alpha_2=0.15$, $M = 35.6 \text{ GPa}$.

Poroelastic healing tissues properties

4 weeks_ Isotropic solid matrix

- Granular tissue

$$\begin{pmatrix} 2.502 & 2.5 & 0 \\ 2.5 & 2.502 & 0 \\ 0 & 0 & 0.001 \end{pmatrix} \text{ (GPa)}$$

$$\begin{aligned}\phi &= 90\% \\ \alpha_1 &= 0.98 \\ \alpha_2 &= 0.96 \\ M &= 2.2 \text{ MPa} \\ \rho &= 1.01 \text{ g/cm}^2\end{aligned}$$

- Cartilage

$$\begin{pmatrix} 5.98 & 5.3 & 0 \\ 5.3 & 5.98 & 0 \\ 0 & 0 & 0.34 \end{pmatrix} \text{ (GPa)}$$

$$\begin{aligned}\phi &= 80\% \\ \alpha_1 &= 0.98 \\ \alpha_2 &= 0.96 \\ M &= 2.4 \text{ MPa} \\ \rho &= 1.04 \text{ g/cm}^2\end{aligned}$$

- Woven bone

$$\begin{pmatrix} 17.1 & 12.9 & 0 \\ 12.9 & 17.1 & 0 \\ 0 & 0 & 2.1 \end{pmatrix} \text{ (GPa)}$$

$$\begin{aligned}\phi &= 50\% \\ \alpha_1 &= 0.976 \\ \alpha_2 &= 0.955 \\ M &= 2.55 \text{ MPa} \\ \rho &= 1.25 \text{ g/cm}^2\end{aligned}$$

Mesh

